

Analytical Solution to Fundamental Bloch NMR Flow Equations for Non-Zero Porosity Transformation Parameter

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Abstract The Bloch NMR flow equation was transformed into a porous media based on the condition that $\gamma^2 B_1^2(t) \ll \frac{1}{T_1 T_2}$ with transformation constant 'a' which must be positive. Furthermore, an emerging differential equation along the line was also solved for a physical case where $A \neq 0$, using the method of partial integration. It assumed that the parameter 'A' that was a consequence of transforming the fundamental Bloch NMR flow equation into a porous media is not trivial, and thus cannot be ignored. It's been decades since analysis has been done using the porosity derived on an assumption of triviality of this parameter. The interesting thing about our solution is that it encompasses the solution for a trivial 'A' which we believe to be a special case. The solution to this equation is useful in describing physical phenomenon such as permeability and for modelling various other intrinsic factors that affect or influence pore dynamics. The result obtained in this study can have applications in functional magnetic resonance imaging (fMRI), petroleum well design and geological engineering.

Keywords Bloch NMR equation, Magnetic Resonance Imaging, Porosity, Permeability, Partial Integration

1. Introduction

The magnetic properties of nuclei have significant applications in medical imaging and biochemical analysis. These applications are possible because the relaxation properties and the resonance frequency for a nucleus depend upon its environment. Factors such as the presence of chemical bonds, paramagnetic ions, and the rate of flow of fluids influence the magnetic resonance (MR) signal. Therefore, different regions of a biological sample produce different MR signals (Faulkner et al., 2009, Hendee et al., 2003). To investigate the transport process of fluid through a small sized pore, say a nanopore, we have to take the surface porosity of the material into consideration as well as other parameters that are intrinsic to the material (Awojoyogbe et al., 2011). Porosity is a term that is used to describe the extent or degree to which a surface perforated with holes can allow small particles to pass or move through it. Porosity as a property can be explored in the creation of bulk micromachining to fabricate tiny cell-containing chambers

within single crystalline silicon wafers. The chambers interface with the surrounding biological environment through polycrystalline silicon filter membranes that are micro machined to present a high density of uniform nanopores as small as 20 nanometres in diameter (Riegler J et al., 2010). These pores are large enough to allow small molecules such as oxygen, glucose, and insulin to pass but are small enough to impede the passage of much larger immune system molecules such as immunoglobulin and graft-borne virus particles (Borchardt et al., 2010). Permeability on the other hand is the ease with which an ion crosses the membrane and is proportional to the total number of open channels for the ion. When two or more ions contribute to the membrane potential, it is likely that the membrane potential would not be at the equilibrium potential for any of the contributing ions. Thus, no ion would be at its equilibrium (i.e., $V_{eq} \neq V_m$). When an ion is not at its equilibrium, an electrochemical driving force (V_{DF}) acts on the ion, causing the net movement of the ion across the membrane down its electrochemical gradient. The driving force is quantified by the difference between the membrane potential and the ion equilibrium potential ($V_{DF} = V_m - V_{eq}$) (Awojoyogbe et al., 2002).

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2. The NMR Flow Equation

In accordance with Awojoyogbe et.al, 2009, the time dependent modified Bloch Nuclear magnetic Resonance (NMR) equations could be obtained from:

$$\frac{d^2 M_y}{dt^2} + T_0 \frac{dM_y}{dt} + (T_g + \gamma^2 \beta^2_1(t)) M_y = \frac{M_0 \gamma \beta_1(t)}{T_1} \quad (1)$$

Based on the condition:

$$\gamma^2 \beta^2_1(t) \ll \frac{1}{T_1 T_2} \Rightarrow \gamma^2 \beta^2_1(t) \ll T_g$$

Then equation (1) becomes:

$$\frac{d^2 M_y}{dt^2} + T_0 \frac{dM_y}{dt} + T_g M_y = \frac{M_0 \gamma \beta_1(t)}{T_1} \quad (2)$$

Where $T_0 = \frac{1}{T_1} + \frac{1}{T_2}$ and T_1 and T_2 are the Spin-Spin and Spin-Lattice relaxation times respectively. M_y is the Transverse Magnetization, γ is the gyro-magnetic ratio and B_1 is the external magnetic field.

3. The Transformation of NMR Transverse Magnetization into a Porous Medium

We apply transformation that will make $M_y(t)$ Expressible in term of $M_y(p)$. This condition transforms $M_y(t)$ into a porous medium with porosity $P(t)$, such that by using total differential, we have:

$$\frac{dM_y}{dt} = \frac{dM_y}{dp} \frac{dp}{dt} \quad (3)$$

And using the product rule, the second derivative can be derived thus:

$$\frac{d^2 M_y}{dt^2} = \frac{d}{dp} \left(\frac{dM_y}{dp} \frac{dp}{dt} \right) \frac{dp}{dt}$$

This becomes:

$$\begin{aligned} \frac{d^2 M_y}{dt^2} &= \left(\frac{d^2 M_y}{dp^2} \frac{dp}{dt} \right) \frac{dp}{dt} + \frac{dM_y}{dp} \left(\frac{d}{dp} \left(\frac{dp}{dt} \right) \frac{dp}{dt} \right) \\ \frac{d^2 M_y}{dt^2} &= \frac{d^2 M_y}{dp^2} \left(\frac{dp}{dt} \right)^2 + \frac{dM_y}{dp} \frac{d^2 p}{dt^2} \end{aligned} \quad (4)$$

Putting equations 3 and 4 into (2), then we have:

$$\begin{aligned} \frac{d^2 M_y}{dp^2} \left(\frac{dp}{dt} \right)^2 + \frac{dM_y}{dp} \frac{d^2 p}{dt^2} + T_0 \frac{dM_y}{dp} \frac{dp}{dt} + T_g M_y \\ = \frac{M_0 \gamma \beta_1(t)}{T_1} \end{aligned}$$

Dividing through by $\left(\frac{dp}{dt} \right)^2$, then we can have:

$$\begin{aligned} \frac{d^2 M_y}{dp^2} + \frac{\left(\frac{d^2 p}{dt^2} \right)}{\left(\frac{dp}{dt} \right)^2} \frac{dM_y}{dp} + T_0 \frac{\left(\frac{dp}{dt} \right)}{\left(\frac{dp}{dt} \right)^2} \frac{dM_y}{dp} \\ + \frac{T_g}{\left(\frac{dp}{dt} \right)^2} M_y = \frac{M_0 \gamma \beta_1(t)}{T_1 \left(\frac{dp}{dt} \right)^2} \end{aligned}$$

By factorization, we can write that:

$$\begin{aligned} \frac{d^2 M_y}{dp^2} + \left[\frac{\left(\frac{d^2 p}{dt^2} \right)}{\left(\frac{dp}{dt} \right)^2} + T_0 \frac{\left(\frac{dp}{dt} \right)}{\left(\frac{dp}{dt} \right)^2} \right] \frac{dM_y}{dp} \\ + \frac{T_g}{\left(\frac{dp}{dt} \right)^2} M_y = \frac{M_0 \gamma \beta_1(t)}{T_1 \left(\frac{dp}{dt} \right)^2} \end{aligned} \quad (5)$$

Let $A = \left[\frac{\left(\frac{d^2 p}{dt^2} \right)}{\left(\frac{dp}{dt} \right)^2} + T_0 \frac{\left(\frac{dp}{dt} \right)}{\left(\frac{dp}{dt} \right)^2} \right]$ and choosing $P(t)$

such that:

$$a^2 = \frac{T_g}{\left(\frac{dp}{dt} \right)^2} \quad (6)$$

(Awojoyogbe et al., 2009)

Putting equation (6) into (5), we have

$$\frac{d^2 M_y}{dp^2} + A \frac{dM_y}{dp} + a^2 M_y = \frac{a^2 M_0 \gamma \beta_1(t)}{T_g * T_1}$$

$$\frac{d^2 M_y}{dp^2} + A \frac{dM_y}{dp} + a^2 M_y = \frac{a^2 T_1 T_2 M_0 \gamma \beta_1(t)}{T_1}$$

$$\frac{d^2 M_y}{dp^2} + A \frac{dM_y}{dp} + a^2 M_y = a^2 T_2 M_0 \gamma \beta_1(t) \quad (7)$$

Where: M_y is the Transverse Magnetization $P(t)$ Is the Porosity, 'a²' is transformation constant and A is a parameter that can be chosen to be zero or non-zero.

4. Derivation of Porosity

In a quest for exploration evaluation, a solution to equation (6) was presented and dominated Literature. The solution was presented as

$$P = P_o \exp(-T_0 t) \quad (8)$$

Where $T_0 = \frac{1}{T_1} + \frac{1}{T_2}$, P_o is the surface porosity, t is the

time constrained to the condition $A=0$ (Awojoyogbe etal, 2009). However, for years now, it has not been solved for a case where $A \neq 0$.

For permeability evaluations, we need to solve equation (6) for a physical case where the parameter A is non-zero and this is non-trivial. In this paper, we are interested in getting the general solution and expression for the equation (6). We start by re-writing equation (6) such that:

$$\frac{d^2 p}{dt^2} + T_0 \left(\frac{dp}{dt} \right) - A \left(\frac{dp}{dt} \right)^2 = 0 \quad \text{For case } A \neq 0 \quad (9)$$

Now we define a term:

$$m = \left(\frac{dp}{dt} \right) \quad \text{So that } \frac{d^2 p}{dt^2} = \frac{dm}{dt} \quad (10)$$

Substituting equation (10) into equation (9) we can write

$$\frac{dm}{dt} + T_0 m - Am^2 = 0$$

$$\frac{dm}{dt} = Am^2 - T_0 m$$

By rearrangement, we have

$$dm = (Am^2 - T_0 m) dt$$

$$\frac{dm}{(Am^2 - T_0 m)} = dt$$

Integrating both sides of the equation, we have:

$$\int \frac{dm}{(Am^2 - T_0 m)} = \int dt \quad (11)$$

Simplifying the left hand side using partial fraction, then we have:

$$\begin{aligned} \frac{1}{m(Am - T_0)} &\equiv \frac{x}{m} + \frac{y}{Am - T_0} \\ &\equiv x(Am - T_0) + my = 1 \end{aligned} \quad (12)$$

Then we have by equating coefficients that:

$$x = -\frac{1}{T_0} \quad \text{and} \quad y = \frac{A}{T_0} \quad (13)$$

Substituting equation (13) into (12), we have

$$\begin{aligned} \frac{1}{m(Am - T_0)} &= -\frac{1/T_0}{m} + \frac{A/T_0}{(Am - T_0)} \\ \frac{1}{m(Am - T_0)} &= \frac{A}{T_0(Am - T_0)} - \frac{1}{mT_0} \end{aligned} \quad (14)$$

Putting equation (14) back into equation (11)

$$\int \left(\frac{A}{T_0(Am - T_0)} - \frac{1}{mT_0} \right) dm = \int dt$$

$$\frac{1}{T_0} \int \left(\frac{A}{(Am - T_0)} - \frac{1}{m} \right) dm = \int dt$$

$$\frac{1}{T_0} \left(\int \frac{A}{(Am - T_0)} dm - \int \frac{dm}{m} \right) = \int dt$$

$$\frac{1}{T_0} \left(\int \frac{A}{(Am - T_0)} dm - \ln(m) \right) = t + c_1$$

Recalling a general integral rule:

$$\int \frac{f'(m)}{f(m)} dm = \ln f(m)$$

$$\Rightarrow \text{if } : f(m) = (Am - T_0), \text{ then } : f'(m) = A$$

Giving rise to:

$$\frac{1}{T_0} (\ln(Am - T_0) - \ln(m)) = t + c_1$$

$$\frac{1}{T_0} \left(\ln \left(\frac{Am - T_0}{m} \right) \right) = t + c_1$$

But $\ln f(m)^k \equiv k \ln f(m)$

Applying this transformation to the equation above, we have:

$$\ln \left(\frac{Am - T_0}{m} \right)^{\frac{1}{T_0}} = t + c_1$$

Taking the exponential of both sides, we have:

$$\left(\frac{Am - T_0}{m}\right)^{\frac{1}{T_0}} = \exp(t + c_1)$$

$$\left(\frac{Am - T_0}{m}\right)^{\frac{1}{T_0}} = \exp(t) * \exp(c_1)$$

But $\exp(c_1) = K_1 = \text{const} \tan t$

$$\left(A - \frac{T_0}{m}\right)^{\frac{1}{T_0}} = K_1 \exp(t)$$

Raising both sides to the power of T_0

$$A - \frac{T_0}{m} = (K_1 \exp(t))^{T_0}$$

$$\frac{T_0}{m} = A - (K_1 \exp(t))^{T_0}$$

Making m the subject of formula.

$$m = \frac{T_0}{A - (K_1 \exp(t))^{T_0}} \tag{15}$$

Substituting equation (15) into equation (10), we have

$$dp = \frac{T_0}{A - (K_1 \exp(t))^{T_0}} dt$$

Integrating both sides of the equation

$$\int dp = \int \frac{T_0}{A - (K_1 \exp(t))^{T_0}} dt$$

$$\int dp = \int \frac{T_0}{A - K_1^{T_0} * \exp(T_0 t)} dt$$

If $K_1^{T_0} = K_2 = \text{const} \tan t$:, then

$$\int dp = \int \frac{T_0}{A - K_2 \exp(T_0 t)} dt \tag{16}$$

We then define another term:

$$u = \exp(T_0 t)$$

$$\frac{du}{dt} = T_0 \exp(T_0 t)$$

$$dt = \frac{du}{T_0 \exp(T_0 t)} \tag{17}$$

Putting equation (17) into (16), then we have:

$$\int dp = \int \frac{T_0}{A - K_2 u} \left(\frac{du}{T_0 u}\right)$$

$$\int dp = \int \frac{1}{A - K_2 u} \left(\frac{du}{u}\right) \tag{18}$$

Applying partial fraction to equation (18) above,

$$\frac{1}{(A - K_2 u)u} \equiv \frac{w}{u} + \frac{n}{(A - K_2 u)} = 1 \tag{19}$$

$$\Rightarrow w = \frac{1}{A}, n = \frac{K_2}{A} \tag{20}$$

Putting equation (19) and (20) into (18), we have:

$$\int dp = \int \left(\frac{1}{Au} + \frac{K_2}{A(A - K_2 u)}\right) du$$

$$\int dp = \frac{1}{A} \int \left(\frac{1}{u} + \frac{K_2}{(A - K_2 u)}\right) du$$

$$\int dp = \frac{1}{A} \left(\int \frac{du}{u} + \int \frac{K_2 du}{(A - K_2 u)}\right)$$

$$\int dp = \frac{1}{A} \left(\ln u + \int \frac{K_2 du}{(A - K_2 u)}\right)$$

Recall that: $\int \frac{f'(u)}{f(u)} du = \ln f(u)$

$$\int dp = \frac{1}{A} \left(\ln u + \int \frac{K_2 du}{-(K_2 u - A)}\right)$$

$$\int dp = \frac{1}{A} \left(\ln u - \int \frac{K_2 du}{(K_2 u - A)}\right)$$

$$\int dp = \frac{1}{A} (\ln u - \ln(K_2 u - A)) + c_2 \tag{21}$$

Recalling the value of u from equation (3.50b)

$$\int dp = \frac{1}{A} \{\ln[\exp(T_0 t)] - \ln[(K_2 \exp(T_0 t) - A)]\} + c_2$$

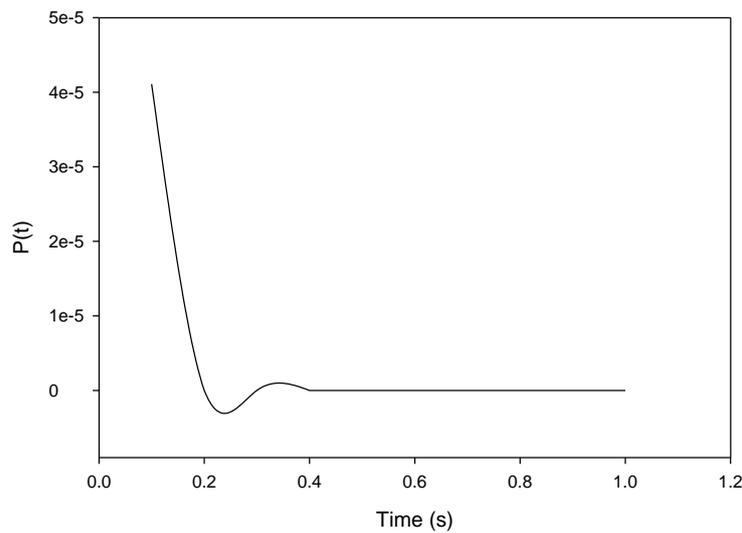
$$p(t) = \frac{1}{A} \{\ln[\exp(T_0 t)] - \ln[(K_2 \exp(T_0 t) - A)]\} + c_2 \tag{22}$$

Equation (22) is the general solution of equation (9) that we are trying to solve for $A \neq 0$. The solution above is the porosity of a porous material as a function of the Magnetic resonance relaxation time (T1 and T2) and the parameter ‘A’, which for many years have been assumed to be zero. The solution above can be a tool to accurately understand the combined effect of the time, relaxation times and the parameter ‘A’ on the dynamics of materials (most especially proteins) through pores. There seems to be evidence to suggest that porosity of a material is not explicitly a function of time only, but something more (Sprawls P., 2000).

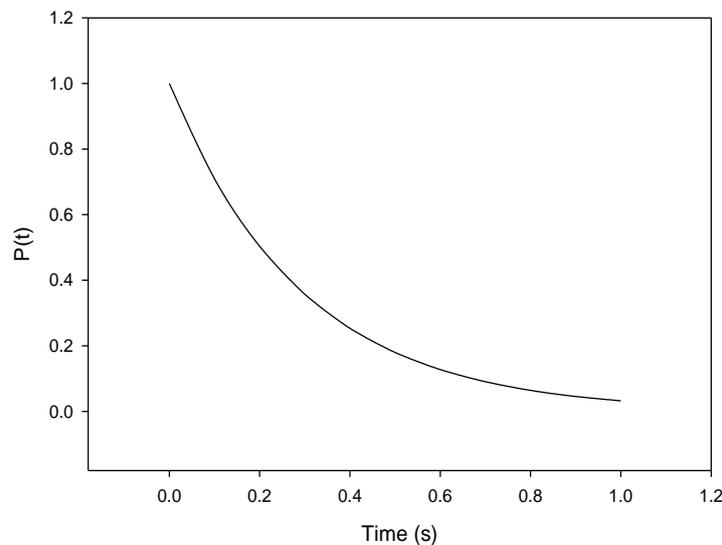
5. Discussion

A simulation of equation (8) and equation (22) is as shown in figure 1(b) and (a) respectively. The choice of T_2 relaxation time was 0.01 sec. which is a typical spin-spin relaxation time for blood flow. Since it was assumed that a nanorobot may move through nanopores as blood will flow through the same porous material (Ottobrini L et al., 2006). From the plot, it is observed that indeed, the parameter ‘A’ has a significant influence on the porosity of a material when imaged through a Magnetic Resonance Imaging (MRI) system. Analysis of equation (8) shows that the porosity $P(t)$ of a nanoporous material varies exponentially with instants of signal sampling and material dependent parameter T_0 , which implies that the porosity of the nanopores decreases at an exponential rate as time of measurement increases, starting from the intrinsic maximum porosity of the material

at time $t=0$ i.e. $P(t)=P_0$. For this research work, P_0 was chosen to be unity (1). The plot of porosity $P(t)$ was made against time to depict the trend of the decay of porosity experienced. Analysis of equation (22) shows that the porosity $P(t)$ oscillates for T_2 relaxation time =0.01 sec while the constant A is chosen to be 5. The porosity was high at an earlier time than 0.2 sec when the oscillation takes place. It is also worthy of note that the presence of parameter ‘A’ has made the porosity to deviate significantly from its intrinsic value at time t close to zero, contrary to what was observed for equation (8). The full wave oscillation was observed between time $t=0.2$ and 0.4 sec. after which the pore closes up for remaining period of observation. The time t for which porosity become measurable increases from 0 to 0.1 sec. This is a consequence of the function of porosity becoming discontinuous at $t=0$.



(a)



(b)

Figure 1. (a) 2 D graph of $P(t)$ and $t(s)$ for equation (22) for $A=5$, $T_2=0.01$, (b) 2 D graph of $P(t)$ and $t(s)$ for equation (8) for $T_2=0.01$

6. Conclusions

We have obtained basic expression for the porosity of a porous material in the light of Magnetic resonance imaging as a function of time, relaxation times and parameter 'A'. This general solution is quite interesting in that in its limiting case, as 'A' tends to zero; equation (22) converges to equation (8) which is ubiquitous in literature. We have also done a computational analysis to have a feeling of how the two solutions differ. The application of this fundamental solution to solve real life problems related to transport in porous and NMR sensitive media will be presented separately. There, we will propose a possible physical meaning of the parameter 'A' and investigate how it affects porosity in combination with other MRI parameters, which is what actually happens in a complex system like human tissue being imaged using MRI.

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